

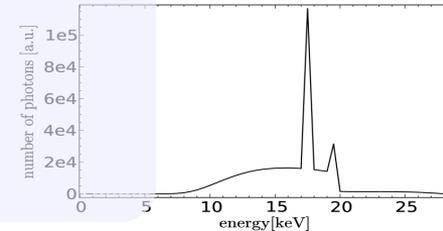
Introduction into brilliant X-ray sources for medical imaging

From X-ray tubes over large-scale synchrotrons to
compact, laser-driven sources

Ultimate goal: dose/contrast agent reduction

➤ disadvantages of x-ray tubes:

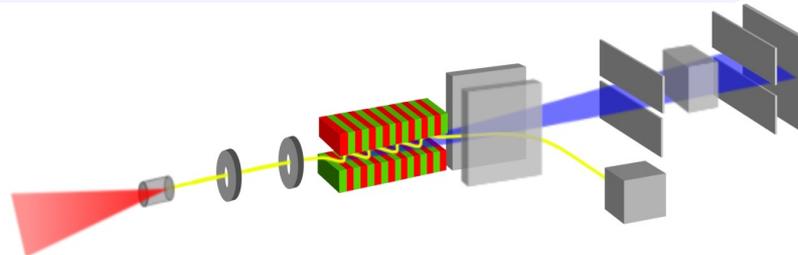
- polychromatic spektrum → low CNR/Dose
- focal spot size → limited spatial resolution (especially for magnification)



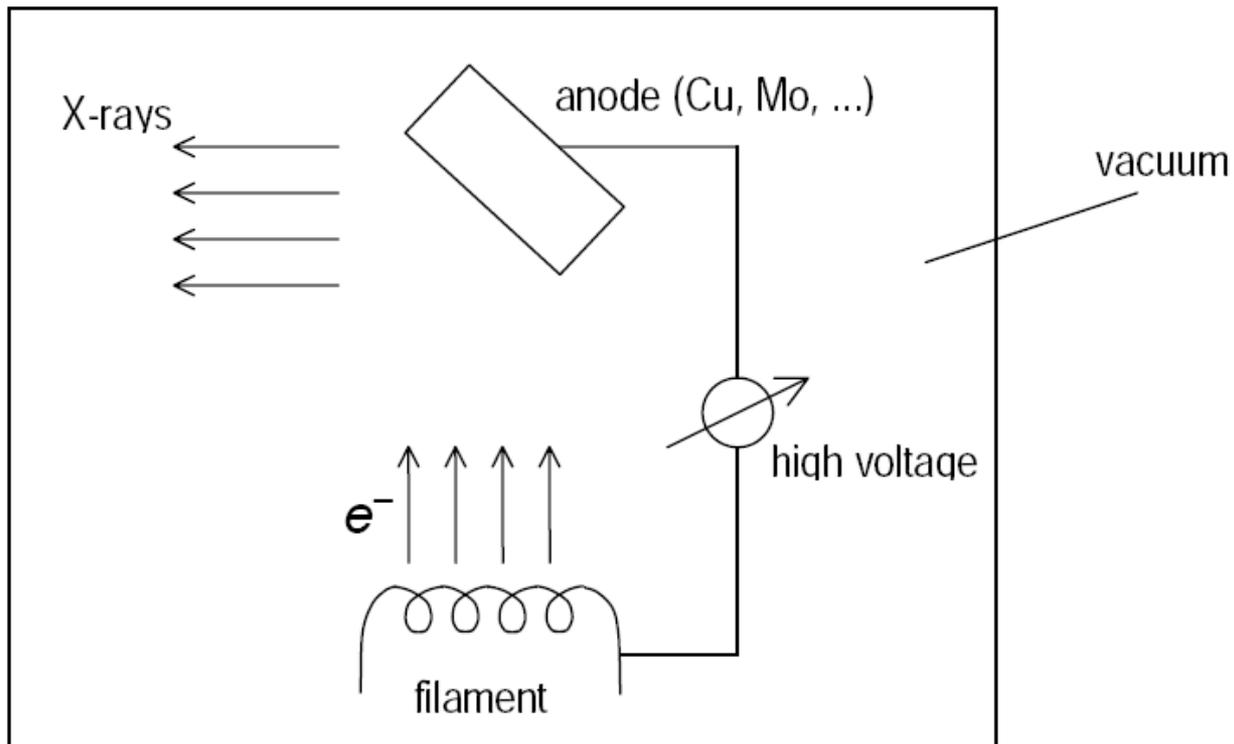
➤ advantages of undulator sources:

- quasi-monochromatic (few %) → **high CNR/dose**
- laminar beam geometry → **scatter reduction**
- low divergence → **high spatial resolution**
- tunable energy

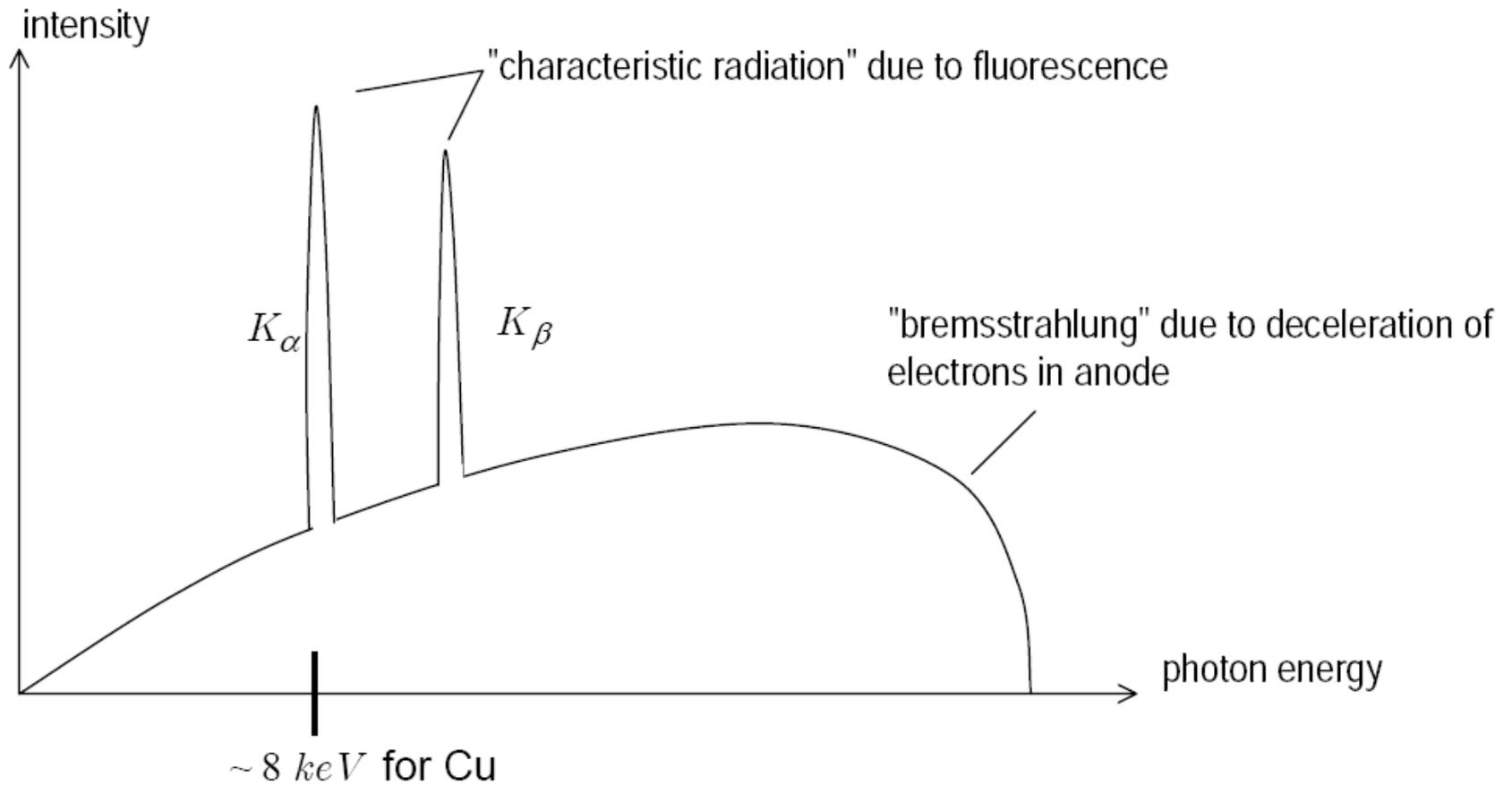
high
brilliance



Laboratory Source ("X-ray tube")



emitted spectrum:



Synchrotron

First constructed for high energy physics experiments since 1970's: dedicated synchrotron sources for condensed matter physics/chemistry/biology (esp. protein crystallography).

Figure of merit for many applications:

$$\text{brilliance} = \frac{\text{photons / sec}}{(\text{mrad})^2 (\text{mm}^2 \text{ source area}) (0.1\% \text{ band width})}$$

↑ 1 ↑ 2 ↑ 3

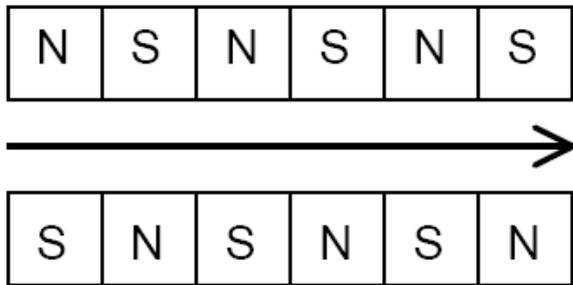
- 1 angular divergence of X-ray beam.
- 2 size of electron beam
- 3 determined by monochromator

Brilliance of synchrotron sources up to $\sim 10^{10}$ larger than X-ray tube, mostly due to much smaller angular divergence. This is important because many experiments use small samples (e.g. protein crystals!) that can use only a tiny fraction of radiation emitted by tube.

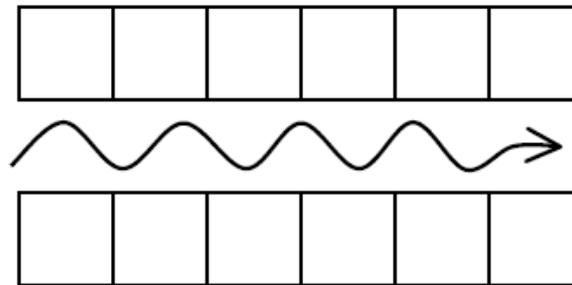
opening angle of synchrotron radiation: $1/\gamma$

► **Wiggler**

side view:



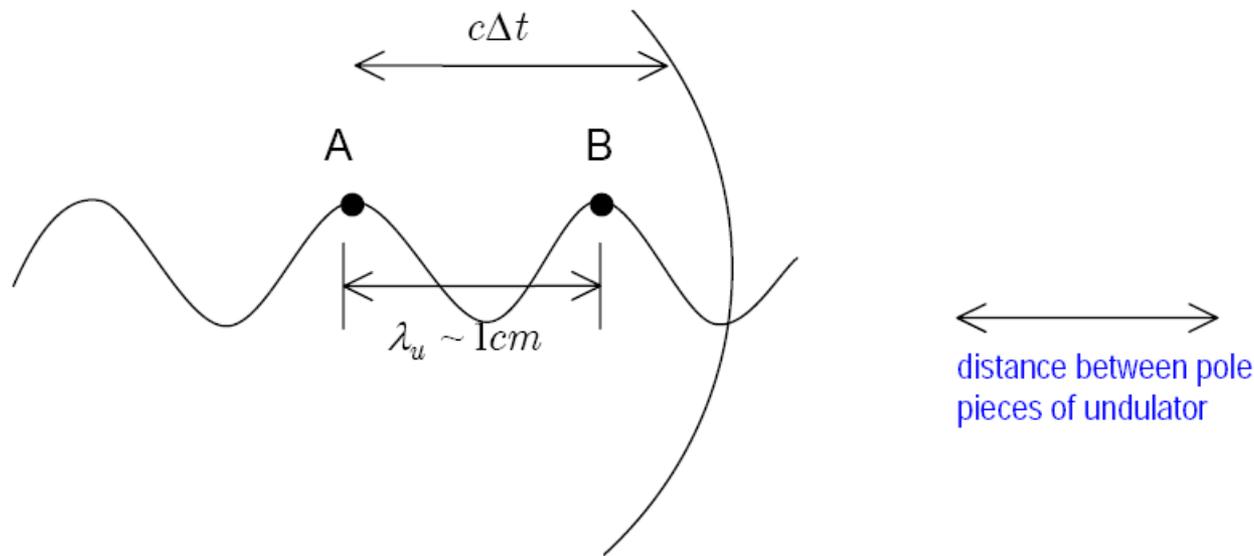
top view:



$N \sim 30$ segments of alternating B-field \Rightarrow intensity enhancement by factor $\sim N$ compared to bending magnet.

► Undulator

Similar to wiggler, but E-fields of wave fronts emitted in each segment are coherent, interfere constructively \Rightarrow intensity enhancement by factor $\sim N^2$.



Time for electron to get from A to B: $\Delta t = \frac{\lambda_u}{v}$

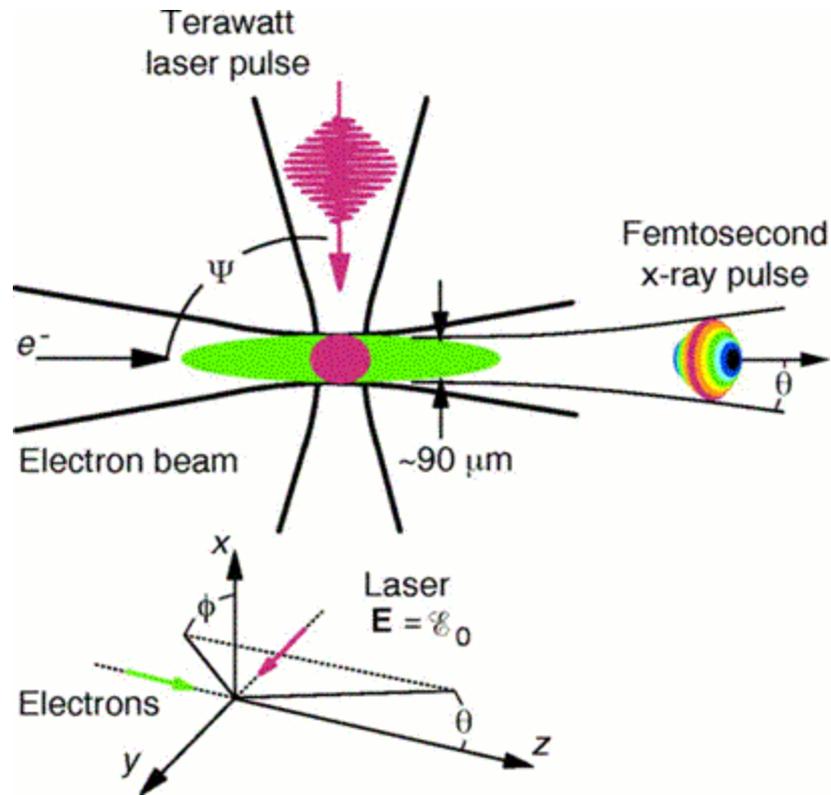
By this time, wave front emitted at A has progressed a distance $c\Delta t$.
Condition for constructive interference:

$$c\Delta t - \lambda_u = n\lambda$$

$$\Rightarrow \left(\frac{c}{v} - 1\right)\lambda_u = \left(\frac{1}{\beta} - 1\right)\lambda_u \approx \frac{\lambda_u}{2\gamma^2} = n\lambda$$

$$\Rightarrow \text{largest intensity at wavelengths } \lambda = \frac{\lambda_u}{2\gamma^2} \frac{1}{n} \sim \frac{1\text{\AA}}{n} \quad (\text{mostly use first harmonic, } n = 1)$$

Laser Thomson scattering equivalent to undulator radiation



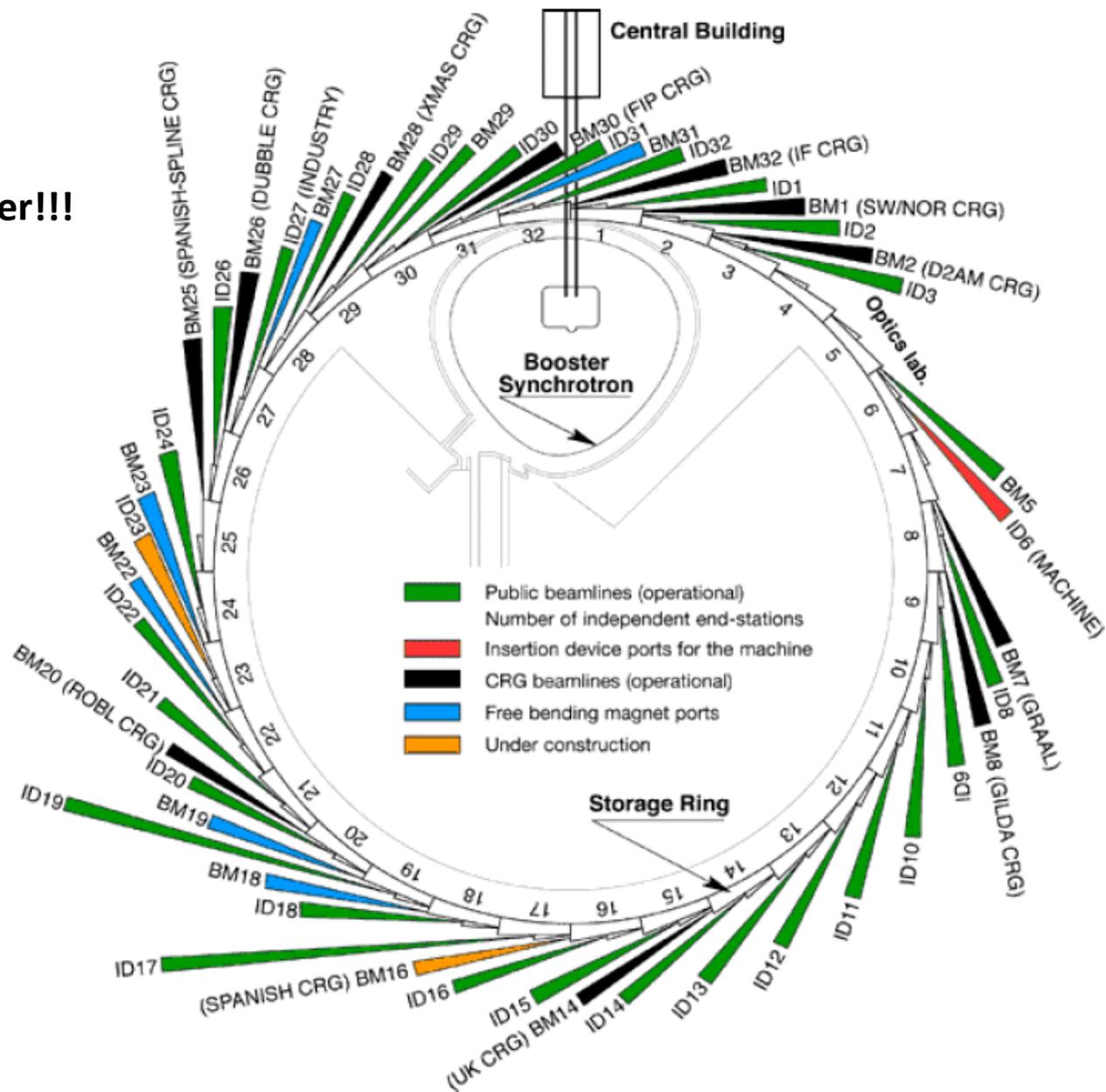
$$\lambda = \frac{\lambda_u}{2\gamma^2}$$

$\lambda_u \rightarrow \lambda_{\text{laser}}$

$2\gamma^2 \rightarrow 4\gamma^2$ as laser moves with $v=-c$, while undulator is at rest

typically: about 40 MeV electrons \rightarrow 50 keV photons

600 m diameter!!!



Source: <http://www.esrf.fr>

For a list of the beamlines, see <http://www.esrf.fr/beamline/>

The "brightness" of a light source:

Source
area, S



Angular
divergence, Ω

Flux, F

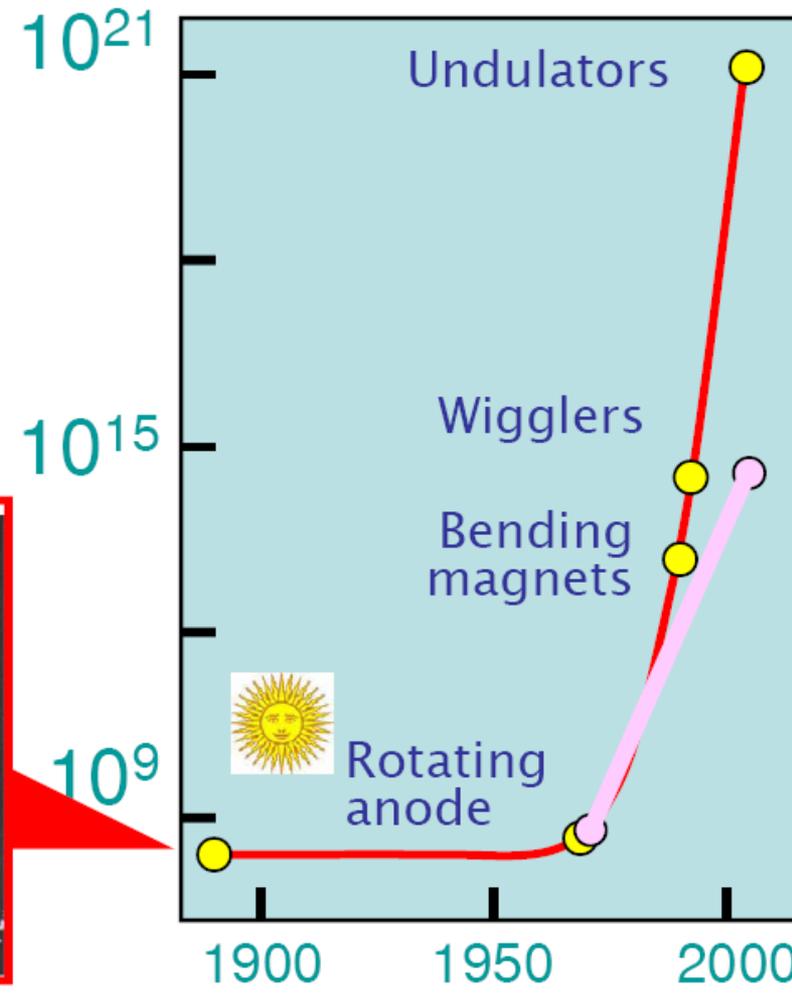
$$\text{Brightness} = \text{constant} \times \frac{F}{S \times \Omega}$$

Steep rise in brightness

the second wave



SLS
SOLEIL (F)
DIAMOND (UK)



ESRF

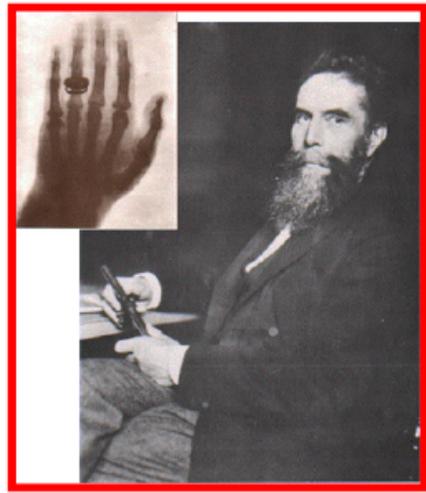


Spring8



APS

Moore's Law for semiconductors



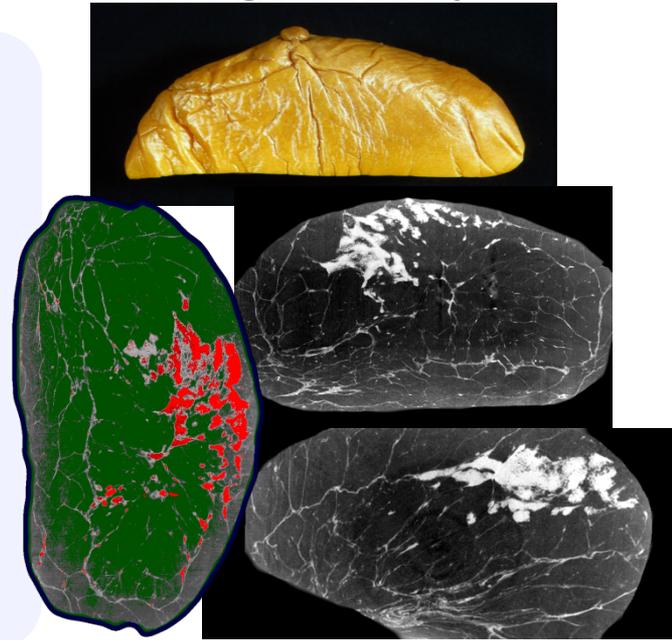
Bertha Roentgen's hand (exposure: 20 min)

Third Generation Light Sources in Operation

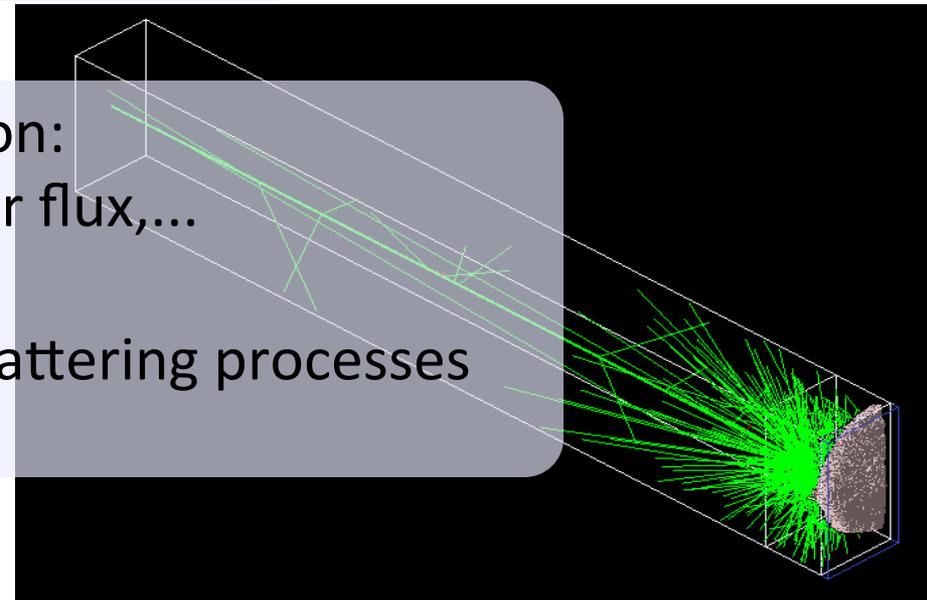


Monte Carlo simulation of mammography

- high resolution voxemodels of breast
- created from CT-scans of anatomical breast specimens
- voxel size: $60 \times 60 \times 60 \mu\text{m}^3$
- segmentation in different tissues:
 - adipose
 - glandular
 - skin



- using **brilliant** undulator radiation: beam geometry, spectral angular flux,...
- pulsed scanning geometry
- simulation of absorption and scattering processes with Geant4-Software-Toolkit



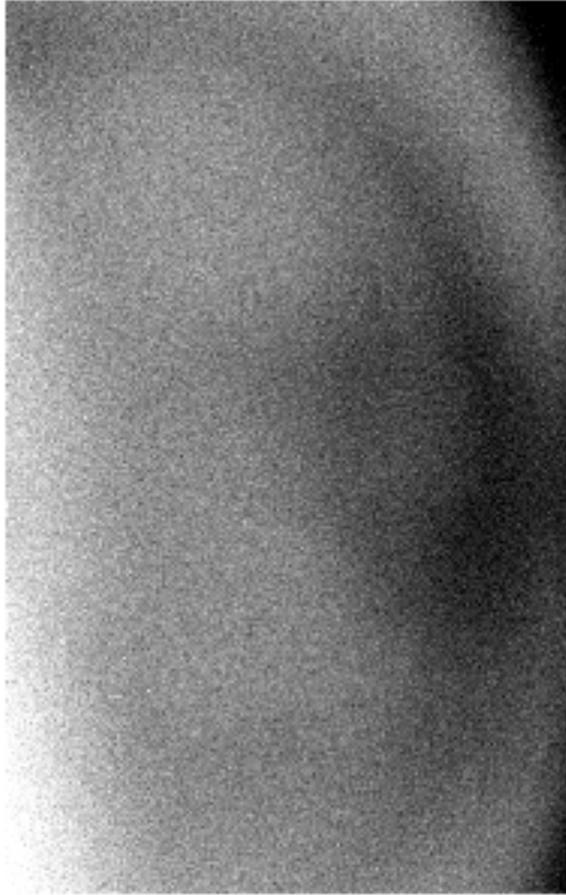
Simulation of mammography

0.2 mGy average glandular dose at $\sim 10^{11}$ photons



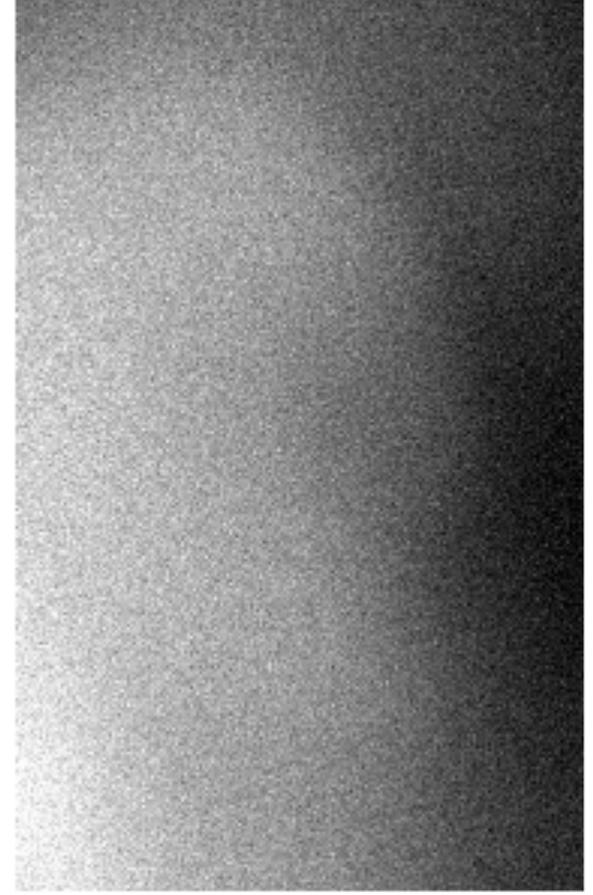
(a)

primary



(b)

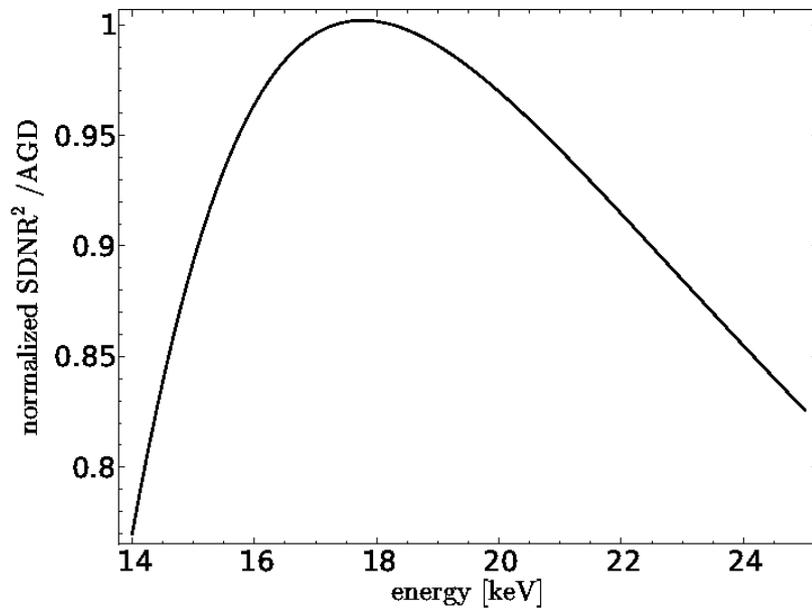
Rayleigh



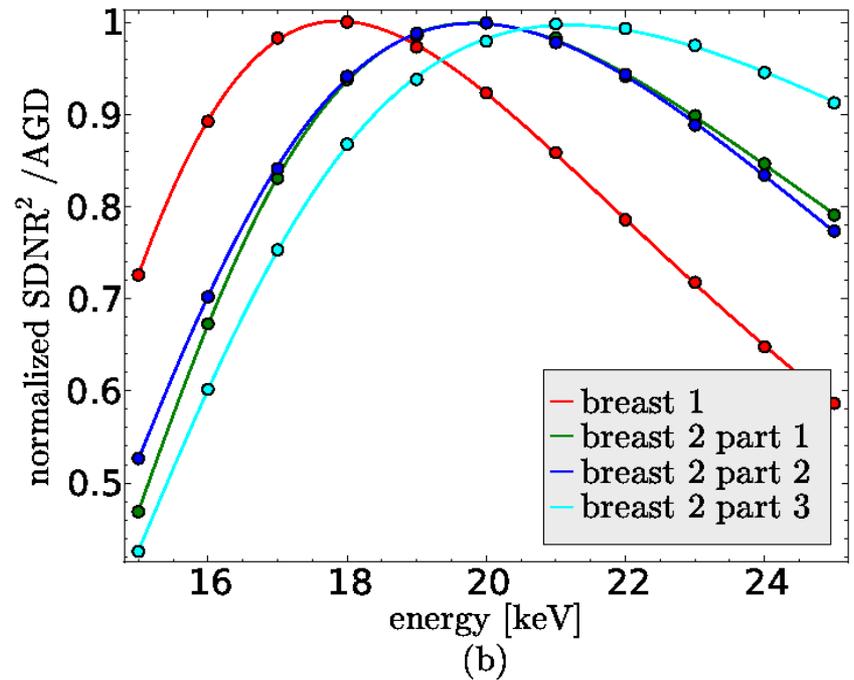
(c)

Compton

optimal X-ray energy



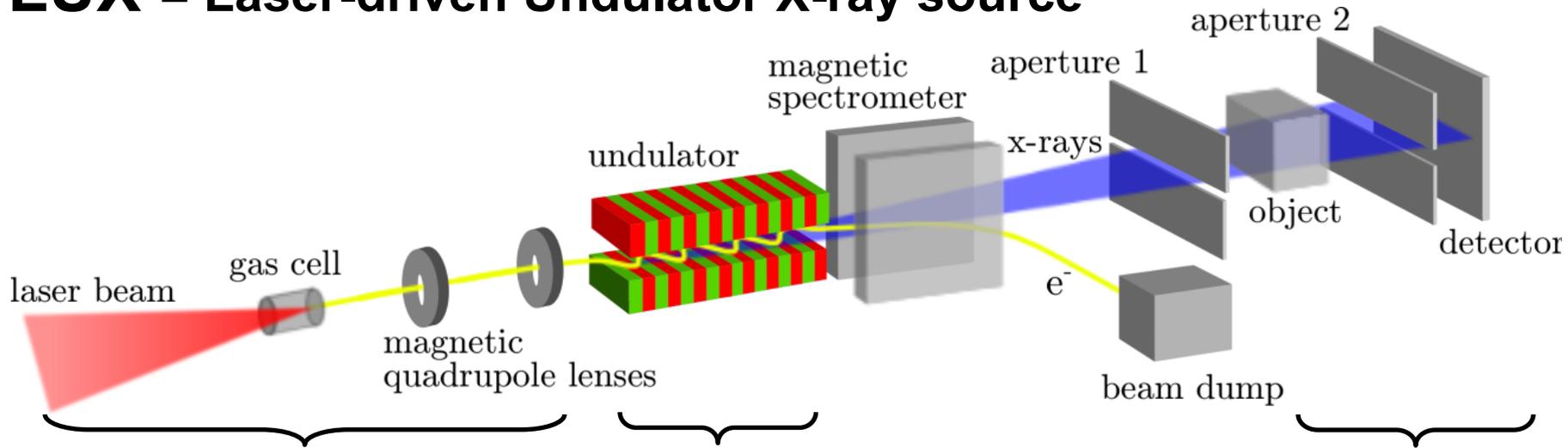
analytical model



simulation for 3 different breast models

→ requires tunable source

LUX = Laser-driven Undulator X-ray source



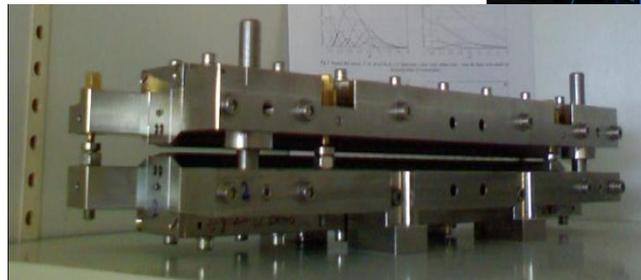
Electron acceleration:

- compact
- stability through band-pass property

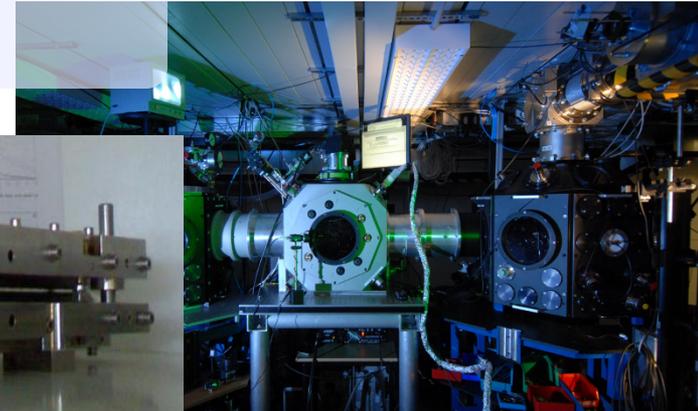


Synchrotron radiation:

- narrow bandwidth
- low divergence



imaging



M. Fuchs et al., Laser-driven soft-X-ray undulator source, Nature Physics 5, 826 (2009)

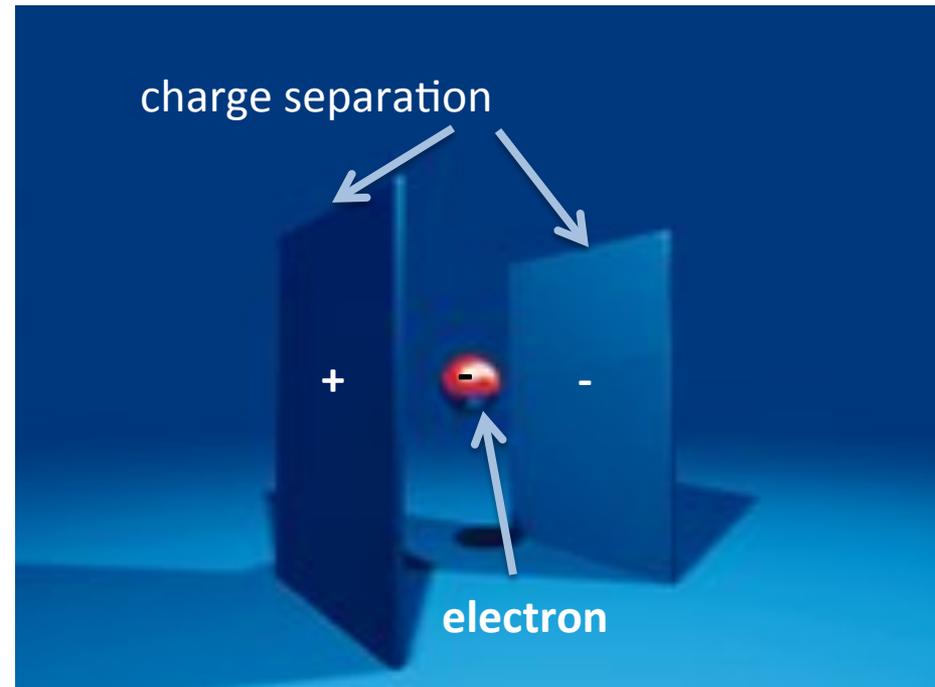
okay up to 25 keV, above one needs Thomson scattering

basic principle of any accelerator

one needs an electric field...



...charged particles are then accelerated



accelerators can be quite large...



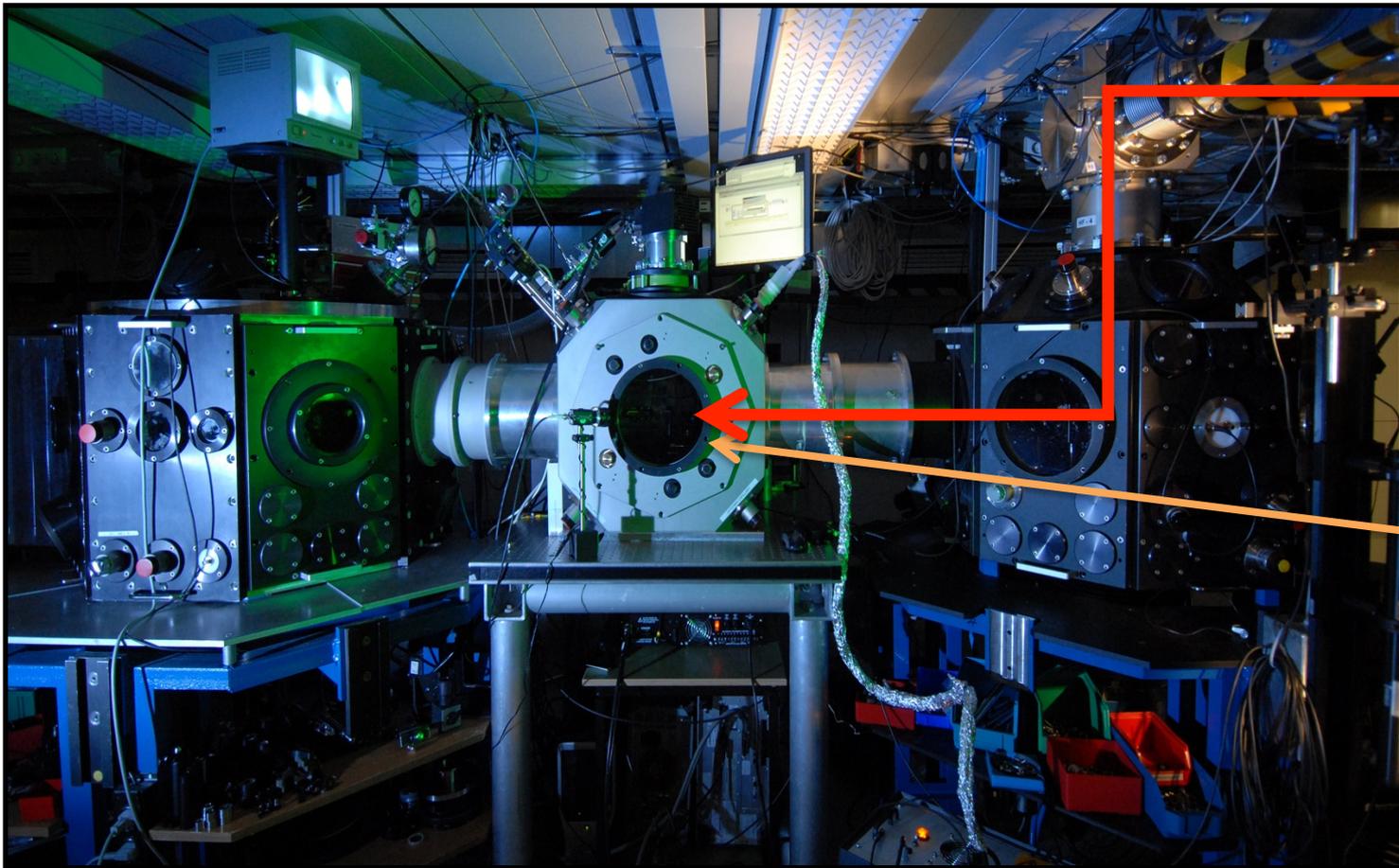
First X-ray FEL (2009):
Stanford, USA

kilometer
long!!!!....

but also quite small...

lab setup of a Laser-Plasma-Accelerator at MPQ (S. Karsch et al.)

pulse of a high-
Power laser



plasma cell:
cm short!!!!...

plasma wakefield acceleration

